

Physics-enhanced velocimetry (PEV) for joint reconstruction and segmentation of noisy velocity images

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Physics-enhanced velocimetry (PEV)





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The material of this presentation is taken from

A. Kontogiannis, S. V. Elgersma, A. J. Sederman, M. P. Juniper, *Joint reconstruction and segmentation of noisy velocity images as an inverse Navier–Stokes problem*, JFM, 944 (A40) 2022.

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Inverse problems in haemodynamics and PC-MRI

- ► PC-MRI measures 4D velocity fields **u**^{*}.
- Measurements become increasingly noisy as spatial resolution is increased.
- To increase SNR, repeated scans are averaged, leading to long signal acquisition times.
- ► PC-MRI signals often need reconstruction.



[Allen et al., J Cardiovasc Magn Reson 2014]

What do we do?

- We use prior information that the image is of a flow through a tube.
- We combine adjoint methods and shape optimization within a Bayesian framework to solve an inverse Navier-Stokes boundary value problem.
- We infer the most likely boundary position, velocity field and viscosity from a PC-MRI signal, obtaining the pressure and wall shear stress for free.

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The Navier-Stokes boundary value problem (e.g. in 2D)





The inverse Navier-Stokes boundary value problem



u^{*} : noisy velocity image

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- u° : reconstruction using an inv. N–S problem (digital twin)
- $\textbf{\textit{u}}^{\star} \mathcal{S} \textbf{\textit{u}}^{\circ}$: noise/artefacts that we filter out
- $\Gamma \qquad \qquad : {\rm most\ likely\ boundary\ of\ the\ object\ } \Omega$

Denoising and improved wall-shear rate estimation

We address two shortcomings of PC-MRI:

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- i. SNR decreases as spatial resolution increases,
- ii. partial volume effects reduce signal near the boundaries,

which hinder the accurate estimation of wall shear stresses.



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(a) Synthetic data \pmb{u}^{\star}



(d) TV-B $\lambda/\lambda_0=0.1$



(b) Our reconstruction $\textbf{\textit{u}}^\circ$



(e) TV-B $\lambda/\lambda_0 = 0.01$



(c) Ground truth \pmb{u}^\bullet



(f) TV-B $\lambda/\lambda_0=0.001$

Figure: Streamlines in the simulated 2D model of an aortic aneurysm (Re = 500).



(a) Zeroth iteration p_0



(d) Zeroth iteration $(\gamma_w)_0$



(b) Our reconstruction p°



(e) Our reconstruction γ_w°



(c) Ground truth p^{\bullet}



(f) Ground truth $\gamma^{\bullet}_{\scriptscriptstyle W}$

Figure: Inferred wall shear stress and pressure.

Work in progress (porous media flows)



(a) Segmented geometry of a packed bed (b) Simulated flow through the packed bed

Figure: Demonstration of the parallel 3D Navier–Stokes (immersed-boundary finite element) solver that we have developed in a packed bed geometry.

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Work in progress (cardiovascular flows)



(a) Segm. geom. of an aortic arch replica



(b) PC-MRI of flow through the replica

Figure: High-quality PC-MRI experiment for the flow through an aortic arch replica (3D-printed model of an aortic arch scanned with CT).

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Work in progress (cardiovascular flows)



(a) 3D experimental (noisy/sparse) PC-MRI



(b) 3D simulated aorta flow

Figure: 3D steady flows in complex geometries from (a) PC-MRI experiments and (b) the Navier-Stokes boundary value problem.

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Conclusions

Summary

We solve an inverse Navier-Stokes boundary value problem for the reconstruction of PC-MRI signals and simultaneously infer the wall-shear stress and pressure.

Why is this trustworthy?

- The data is assimilated into a model that is hard-wired to satisfy the Navier-Stokes equations. Uncertainties are rigorously quantified. There is no image processing, no neural network and no training data.
- The Navier-Stokes model can be complemented by viscosity models for blood, although this is unlikely to be necessary for vessels visible with MRI.
- Compared with current methods, this method requires around 100 times less data to extract the same flow information.

What's next?

- We will extend the method to 3D geometries and 4D periodic flows.
- ▶ We will reconstruct PC-MRI data of *in-vivo* cardiovascular flows.

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